

1 **High-expanding regions in primate cortical brain evolution support**
2 **supramodal cognitive flexibility**

3 Markus H. Sneve^{1*}, Håkon Grydeland¹, Marcello G. P. Rosa^{2,3,4}, Tomáš Paus^{5,6,7,8}, Tristan
4 Chaplin^{2,3,4}, Kristine Walhovd^{1,9}, & Anders M. Fjell^{1,9}

5

6 ¹Center for Lifespan Changes in Brain and Cognition, Department of Psychology, University of Oslo,
7 Oslo, Norway

8 ²Department of Physiology, Monash University, Clayton, VIC 3168, Australia

9 ³Biomedicine Discovery Institute, Monash University, Clayton, VIC 3168, Australia

10 ⁴Australian Research Council, Centre for Excellence for Integrative Brain Function, Monash
11 University, Clayton, VIC 3168, Australia

12 ⁵Rotman Research Institute, University of Toronto, Toronto, Canada M6A 2E1

13 ⁶Department of Psychiatry, University of Toronto, Toronto, Canada M5S 1A1

14 ⁷Center for Developing Brain, Child Mind Institute, New York, NY 10022, USA

15 ⁸Department of Psychology, University of Toronto, Toronto, Canada M5S 1A1

16 ⁹Department of Radiology and Nuclear Medicine, Oslo University Hospital, Oslo, Norway

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18 Address correspondence to:

19 Markus Handal Sneve, Dept. of Psychology. Pb. 1094 Blindern, 0317 Oslo, Norway

20 Phone: +47 22 84 52 16; E-mail: m.h.sneve@psykologi.uio.no

21

22 **Abstract**

23 Primate cortical evolution has been characterized by massive and disproportionate
24 expansion of a set of specific regions in the neocortex. The associated increase in neocortical
25 neurons comes with a high metabolic cost, thus the functions served by these regions must
26 have conferred significant evolutionary advantage. In the present series of analyses, we
27 show that evolutionary high-expanding cortex – as estimated from patterns of surface
28 growth from several primate species – shares functional connections with different brain
29 networks in a context-dependent manner. Specifically, we demonstrate that high-expanding
30 cortex is characterized by high internetwork functional connectivity; is recruited flexibly over
31 many different cognitive tasks; and changes its functional coupling pattern between rest and
32 a multimodal task-state. The capacity of high-expanding cortex to connect flexibly with
33 various specialized brain networks depending on particular cognitive requirements suggests
34 that its selective growth and sustainment in evolution may have been linked to an
35 involvement in supramodal cognition. In accordance with an evolutionary-developmental
36 view, we find that this observed ability of high-expanding regions – to flexibly modulate
37 functional connections as a function of cognitive state – emerges gradually through
38 childhood, with a prolonged developmental trajectory plateauing in young adulthood.

39

40

41 **Keywords**

42 cerebral cortex, functional connectivity, human brain evolution, human development, multi-
43 modal integration

44 The most striking feature of the human brain when compared with brains of other primates,
45 is its massively expanded cerebral cortex, mainly due to a higher number of cortical neurons
46 (Herculano-Houzel 2012; Buckner and Krienen 2013). The growth of the primate cortex has
47 not been uniform, however, with a set of so-called 'hotspot' regions in lateral temporal,
48 parietal and prefrontal cortex showing disproportionately high expansion (Hill et al. 2010;
49 Chaplin et al. 2013). Well-supported models suggest that this non-uniform growth has
50 followed allometric scaling laws, and that the massive expansion of certain regions in
51 evolution therefore is a predicted consequence of growing a bigger brain (Finlay and
52 Darlington 1995; Toro et al. 2008; Herculano-Houzel 2012; Chaplin et al. 2013; Rilling 2014;
53 Amlien et al. 2016; although see e.g. Smaers et al. 2017). Nevertheless, the metabolic costs
54 associated with sustaining a higher number of neurons are high (Ringo 1991; Herculano-
55 Houzel 2011) and impose limitations on the growth of other, non-neuronal, physical
56 capacities such as body size (Fonseca-Azevedo and Herculano-Houzel 2012). An intriguing
57 question is therefore: what functions do high-expanding regions in primate brain evolution
58 serve, which may have offset these potential natural selection costs?

59

60 Expansion 'hotspots' refer to the cortical regions that differ the most between extant
61 primates of different brain sizes (Chaplin et al. 2013) and are considered a useful proxy for
62 the parts of cortex that have undergone the most expansion during evolution (Hill et al.
63 2010; Buckner and Krienen 2013). As prototypical members of association cortex, these
64 evolutionary high-expanding regions are involved in various tasks and functional systems
65 and have been theorized to serve relational reasoning and integrative higher-order cognition
66 (Krienen et al. 2014; Vendetti and Bunge 2014). In support of these views, measures of
67 general cognitive abilities in human adults have been shown to correlate positively with

68 cortical surface-area within high-expanding regions (Fjell et al. 2015), associations not found
69 within low-expanding cortex (Vuoksimaa et al. 2016). Furthermore, when compared with
70 brain regions showing less evolutionary expansion, high-expanding cortex shows higher
71 growth of the surface area during human development (Hill et al. 2010; Amlien et al. 2016),
72 and this pattern is more pronounced in individuals with high intelligence (Schnack et al.
73 2015).

74

75 In the current study, we tested the hypothesis that the growth and sustainment of high-
76 expanding cortex has facilitated supramodal cognition (Goldman-Rakic 1988),
77 conceptualized as the integration of information from across the brain in a flexible manner.
78 By taking advantage of recent developments in brain network analysis (Rubinov and Sporns
79 2010), and applying these to histological data and magnetic resonance imaging (MRI) scans
80 of multiple primate brains, as well as a large sample of humans during different cognitive
81 states and at different stages in development, we were able to directly test the predictions
82 that high-expanding cortex 1) has broad functional connections with different specialized
83 brain networks; 2) is flexibly engaged by a diverse set of cognitive tasks; 3) is more central to
84 communication flow in the brain during states requiring multimodal integration than during
85 low-demand states; 4) increases functional coupling preferentially with regions engaged by
86 the current cognitive demands. Moreover, given the correlation between morphological
87 changes in primate brain evolution and human development, we predict that the functional
88 connectivity patterns associated with supramodal cognition develop gradually, and fully
89 emerge relatively late in postnatal life.

90 **Materials and Methods**

91 **Human subjects**

92 RsfMRI-data were collected in 221 healthy young adults (age range 18-38, mean age 23.8;
93 142 females). Task-fMRI data were collected in 105 of the same participants (age range 18-
94 38, mean age 25.3; 69 females), as well as in 46 children and adolescents (age range 6-17,
95 mean age 12.9; 21 females). The study was approved by the Regional Ethical Committee of
96 South Norway, and participants provided written informed consent. Participants were
97 required to be right-handed, speak Norwegian fluently and have (corrected to) normal
98 hearing and vision. Clinical sequences (T2-FLAIR) were inspected by a neuroradiologist and
99 deemed free of significant injuries or conditions.

100

101 **Non-human primates**

102 Evolutionary cortical expansion was calculated from the brains of four simian primates:
103 marmoset (*Callithrix jacchus*), capuchin (*Cebus apella*), macaque (*Macaca mulatta*) and
104 human. Details about the calculations have been described in a previous publication (Chaplin
105 et al. 2013). Briefly, surface models of the cerebral cortex of the four species were registered
106 by deforming the models to align a set of landmarks, consisting of well-established
107 homologous cortical regions, using the CARET software package (Van Essen et al. 2001).
108 Expansion was calculated as the change in size of each mesh polygon, and was averaged
109 across the marmoset to capuchin, marmoset to macaque, and macaque to human
110 deformations. All tests involving comparisons with evolutionary expansion were restricted to
111 measures extracted from right-hemispheric nodes. For the "State-dependent coupling
112 analyses" (Fig. 2), and the "Developmental sample analyses" (Fig. 3), cortical nodes were

113 binned per evolutionary expansion (SFig. 5). We considered the 20% highest-expanding
114 nodes 'hotspot' regions, and this definition revealed three separate clusters commonly
115 discussed in the literature (Hill et al. 2010; Chaplin et al. 2013).

116

117 **Experimental design**

118 Resting-state fMRI was collected during eyes-closed rest. Participants were instructed to not
119 fall asleep. Given recent reports that eyes-closed resting-state is associated with higher
120 levels of unintentional sleep among participants when compared to eyes-open rest
121 (Tagliazucchi & Laufs, 2014), the current sample only included participants that confirmed
122 compliance and reported that they remained awake throughout the scan. During the fMRI-
123 task, participants sequentially viewed 100 line drawings of objects and immediately
124 produced a motor response indicating whether the object was congruent with a spoken
125 action (either "Can you eat it" or "Can you lift it"; SFig. 3). The task is described in detail
126 elsewhere (Sneve et al. 2015).

127

128 **MRI acquisition**

129 Imaging was performed at a Siemens Skyra 3T MRI unit with a 24-channel head coil. For the
130 fMRI scans (rest and task), 43 slices (transversal, no gap) were measured using T2* BOLD EPI
131 (TR=2390 ms; TE=30 ms; flip angle=90°; voxel size=3x3x3 mm; FOV=224x224; interleaved
132 acquisition; GRAPPA=2). The rsfMRI run produced 150 volumes and lasted ≈6 min. The task
133 data were collected over 2 runs, each consisting of 131 volumes and lasting ≈5.2 min. Three
134 dummy volumes were collected at the start of each fMRI scan to avoid T1 saturation effects
135 in the analyzed data. A standard double-echo gradient-echo field map was acquired for
136 distortion correction of the EPI images. Anatomical T1-weighted MPRAGE images consisting

137 of 176 sagittally oriented slices were obtained using a turbo field echo pulse sequence
138 (TR=2300 ms, TE=2.98 ms, flip angle=8°, voxel size=1×1×1 mm, FOV=256×256 mm).

139

140 **MRI preprocessing**

141 Cortical reconstruction of the T1-weighted scans was performed with Freesurfer 5.3's recon-
142 all routines, and included surface inflation (Fischl et al., 1999a) and registration to a spherical
143 atlas which utilized individual cortical folding patterns to match cortical geometry across
144 subjects (Fischl et al., 1999b). Functional MRI-data were corrected for B0 inhomogeneity,
145 motion and slice timing corrected, and smoothed (5mm FWHM) in native volume space
146 using FSL (<http://fsl.fmrib.ox.ac.uk/fsl/fslwiki>). Next, FMRIB's ICA-based Xnoiseifier (FIX;
147 Salimi-Khorshidi et al. 2014) was used to auto-classify noise components and remove them
148 from the fMRI data. Such ICA-based procedure for denoising fMRI data has been shown to
149 effectively reduce motion-induced variability, outperforming methods based on removing
150 motion spikes in the dataset (Pruim et al., 2015). Importantly, different classifiers were used
151 for rsfMRI and task-fMRI data. Classifiers were trained on scanner-specific datasets in which
152 rsfMRI/task-fMRI data from 16 participants had been manually classified into signal and
153 noise components (fMRI acquisition parameters identical to the current study). Motion
154 confounds (24 parameters) were regressed out of the fMRI data as a part of the FIX routines.
155 Freesurfer-defined individually estimated anatomical masks of cerebral white matter (WM)
156 and cerebrospinal fluid / lateral ventricles (CSF) were resampled to each individual's
157 functional space. Following FIX, average time series were extracted from functional WM-
158 and CSF-voxels and were regressed out of the FIX-cleaned 4D volume. Following recent
159 recommendations (Hallquist et al. 2013) we band-pass filtered the rsfMRI data (.009-.08Hz)

160 after regression of confound variables. Task-fMRI data were detrended and highpass filtered
161 with a .01Hz cutoff.

162

163 **Network analysis of rsfMRI data**

164 A custom cortical parcellation was created in Freesurfer's average surface space (fsaverage),
165 using a modified N-cut algorithm (Craddock et al. 2012), consisting of 340 (170 per
166 hemisphere) spatially contiguous, approximately equally sized nodes covering the entire
167 cerebral cortex. The parcellation was resampled into each participant's functional volume
168 space using a projection factor of 0.5, i.e., half way into the cortical sheet. For each
169 participant, we extracted mean pre-processed rsfMRI time series from all nodes and
170 calculated a 340x340 connectivity matrix consisting of the Pearson's r correlations between
171 nodal time series. Next, we Fisher-transformed all participants' connectivity matrices, and
172 averaged across participants to create a "grand average" connectivity matrix on which
173 network analysis was performed. The grand average connectivity matrix was thresholded at
174 5, 6, 7, 8, 9, 10, 15, and 20% edge densities. For all thresholded weighted graphs, the optimal
175 modular resolution parameter (γ) promoting stable decomposition results, was
176 calculated using the Versatility approach (Shinn et al. 2017; see SFig1). Next, modular
177 decomposition was performed with the Louvain algorithm (Blondel et al. 2008) as
178 implemented in the Brain Connectivity Toolbox (BCT) (Rubinov and Sporns 2010) and
179 followed by consensus clustering (Sporns and Betzel 2016). Briefly, this involved calculating
180 an agreement matrix from 10000 independent Louvain partitions, thresholding this empirical
181 agreement matrix by the maximum agreement observed over 10000 randomly generated
182 null association matrices and running clustering on the thresholded empirical agreement
183 matrix. In the case of singleton partitions, i.e., network modules consisting of one node only

184 – typically consisting of low signal-to-noise regions such as the temporal pole and
185 orbitofrontal cortex – these modules were excluded from the remaining network analyses.
186 Finally, we used the thresholded graphs' optimal community structures to calculate two
187 nodal network measures per graph: *participation coefficient* and *within-module degree*,
188 representing a node's intermodular and intramodular centrality, respectively (Rubinov and
189 Sporns 2010). Two additional measures not requiring information about the underlying
190 community structures were also calculated: *betweenness centrality*, representing the
191 fraction of all shortest paths in the network that contains a given node, and *strength*, the
192 sum of a given node's connectivity weights to every other node (Rubinov and Sporns 2010).
193 Relationships between nodal network measures and estimates of evolutionary expansion
194 were investigated using nonparametric Spearman correlations due to non-normal
195 distributions (assayed using Q-Q plots).

196

197 **Community density analyses**

198 To investigate high-expanding nodes' anatomical centrality, we used a parcellation of human
199 cortical intrinsic connectivity into 17 canonical networks, estimated from 1000 participants
200 (Yeo et al. 2011). First, we extracted MNI-coordinates for every vertex in the right
201 hemisphere in a downsampled Freesurfer surface representation (fsaverage5; 10242
202 vertices). Next, for each vertex, we counted the number of canonical networks present
203 within a radius of 5, 10, 15, 20, 25, and 30mm (Euclidean distance). For each radius, the
204 number of networks at every vertex was normalized (0-1) by the maximum number of
205 networks found across all vertices (Power et al. 2013). Finally, the normalized community
206 density values were averaged across radii at each vertex, and correlated with evolutionary

207 expansion estimates at the same locations using Spearman correlations (due to non-normal
208 distributions).

209

210 **Flexibility analyses**

211 The functional flexibility of each vertex on the cortical surface of the right hemisphere was
212 estimated from publicly available data
213 (https://surfer.nmr.mgh.harvard.edu/fswiki/BrainmapOntology_Yeo2015). Here, an author-
214 topic hierarchical Bayesian model was used to classify 10449 experimental contrasts from
215 fMRI experiments found in the BrainMap database (Fox and Lancaster 2002) into 12
216 underlying cognitive components and corresponding brain activity patterns (Yeo et al. 2015).
217 Flexibility was defined as the number of cognitive components activating a voxel. To account
218 for non-integer values due to projections from volume to surface space we rounded surface
219 flexibility estimates to the nearest integer. A nonparametric Kruskal-Wallis was used to
220 compare central tendencies in evolutionary expansion across flexibility groups due to
221 unequal variances across groups (significant Bartlett's test: $\chi^2(8) = 3549, p < 1e-10$)

222

223 **Task-state connectivity**

224 Following preprocessing, volumetric task-fMRI data were brought to fsaverage surface
225 space. Here, for each participant, we extracted mean BOLD time series from all nodes in the
226 custom 340-node cortical parcellation. Next, psychophysiological interaction (PPI) terms
227 representing nodal task-related activity modulations were calculated using the generalized
228 PPI-toolbox for Matlab (McLaren et al. 2012). For each node, this involved: 1) deconvolving
229 the mean BOLD time series into estimates of neural events (Gitelman et al. 2003); 2) setting
230 up a task-regressor representing the combined auditory-visual-motor-event (2s trial

231 duration, 50 trials per fMRI run) 3) convolving the product of step 1 and 2 with a canonical
232 hemodynamic response function (cHRF). Finally, to establish task-related functional
233 connectivity between nodes, we estimated pairwise interactions between all nodes' PPI-
234 terms (concatenated over runs) using partial correlations. For each pairwise correlation, we
235 controlled for background noise and task stimulation effects using the nodes' mean BOLD
236 time series and the cHRF-convolved task-regressor, respectively. This "correlational PPI"
237 approach has been described in detail elsewhere (Fornito et al. 2012).

238

239 **State-dependent coupling analyses**

240 A total of 105 adult participants were represented with matrices of functional connectivity
241 obtained from a resting-state and a task-state. First, the individual connectivity matrices
242 were thresholded to contain only edges surviving FDR-correction ($q < .05$). Next, to allow for a
243 comparison of connectivity data from different states, edge-wise connectivity weights were
244 normalized by the average weight in the matrix (Opsahl et al. 2010). After mapping from
245 weights to lengths (inverting the connection-weights matrices), shortest path-lengths were
246 calculated using Dijkstra's algorithm (Dijkstra 1959). A node's closeness centrality was
247 calculated as the inverse of the average of its shortest path-length to every other node. A
248 repeated measures ANOVA with two within-subject factors; "expansion bin" (5 levels) and
249 "state" (2 levels); was performed to compare closeness centrality measures over regions
250 having undergone different amount of expansion in evolution, as a factor of cognitive state.
251 Note that although estimates of functional connectivity from the two states were derived
252 using different approaches (rest: timeseries correlations; task: correlational PPI), both
253 approaches involve calculating the Pearson's correlation coefficient between the regions'
254 ongoing spontaneous BOLD fluctuations during periods of interest. The state comparisons

255 were also conducted using identical pre-processing and analysis approaches across the
256 states (see "Control Analyses" below).

257

258 **Analyses of the developmental sample**

259 The developmental sample consisted of the 105 adult participants described in the section
260 "State-dependent coupling analyses" and 46 participants below 18 years of age (see "Human
261 subjects" section). All non-adult participants were preprocessed and analyzed as described
262 for the adult sample. One participant (age 9.3 years) was excluded from the sample due to
263 high levels of motion (mean absolute motion over two task runs > 1.5mm). A significant
264 positive correlation (Spearman's $\rho = .37, p < 4e-06$) was found in the remaining
265 developmental sample (N=150) between estimated motion during the task-state (first
266 principal component of mean absolute and relative motion over two task runs, explaining
267 98.1% of the total variance) and global closeness centrality (average closeness centrality
268 over all 170 nodes, corresponding to the graph theoretical measure global efficiency
269 (Rubinov and Sporns 2010)). This positive correlation between subject motion and global
270 closeness centrality indicated that participants with relatively high levels of motion (which is
271 a characteristic of young samples (Satterthwaite et al. 2012)) also tended to show high
272 estimates of closeness centrality. To allow for comparisons of closeness-centrality estimates
273 across age groups, unbiased by motion at the global level, we therefore standardized (z-
274 scored) the estimates on a within-subject basis before comparing relative coupling
275 differences across groups. This effectively removed all correlations with motion also when
276 investigating high-expanding and lower-expanding cortex separately (Spearman's ρ
277 calculated over five expansion bins; lowest expansion to highest expansion: -.06, .14, -.04,

278 .04, -.01; all p -values > .09). Furthermore, we included individual estimates of mean absolute
279 and relative motion as covariates in all statistical tests.

280

281 To compare relative coupling across age groups, a repeated measures ANOVA was run with
282 one within-subject factor: "expansion bin" (5 levels), and one between-subject factor: "age
283 group" (2 levels). Mean absolute and relative motion over two task runs were included as
284 covariates. Next, for all 150 participants in the developmental sample, we calculated task-
285 state closeness centrality for each of the 170 nodes in the custom right hemisphere
286 neocortical parcellation and correlated these with evolutionary expansion estimates for the
287 same nodes. We then fitted a nonparametric local smoothing model minimizing the
288 Bayesian information criterion (BIC) to delineate the age trajectory of the relationship
289 between closeness centrality and evolutionary expansion (Fjell et al. 2010). Note that the BIC
290 of the optimal smoothing spline was 8.7 lower than the BIC of a linear fit, indicating that the
291 age trajectories were curvilinear. Confidence intervals of the fit were established using
292 bootstrapping.

293

294 Scores on the matrix reasoning and vocabulary subtests of the Wechsler's Abbreviated Scale
295 of Intelligence (WASI; Wechsler 1999) were available from 140 of the participants in the
296 developmental sample (age range 7-38 years). Principal component analysis was run on the
297 raw scores of the two subtests, and the first component, which explained 95.5% of the total
298 variance, was used as a representative measure of general intelligence across participants.

299

300 **Weighting by Euclidean distance**

301 Euclidean distance between nodes in the right hemisphere was calculated as the average
302 distance (in mm) between the locations of their constituent vertices converted to MNI305
303 space. To calculate the weighted connectivity matrices, the Euclidean distance matrix was
304 normalized to fall between 0 and 1 and multiplied, element-by-element, with the
305 connectivity matrices across states and participants. Such weighting by geometric distance
306 has been shown to increase sensitivity in detecting graded network differences (Liu et al.,
307 2014), and was applied in all analyses performed on the single-subject level involving
308 comparisons between states or individuals (i.e., the state-dependent coupling analyses
309 (Fig.2), and the analyses of the developmental sample (Fig. 3)). As the network analyses of
310 the rsfMRI data (Fig. 1b) were performed on the grand-average graph and required
311 community detection steps (for which distance weighting would produce networks not
312 comparable to those typically shown in the literature), we conducted these analyses on
313 unweighted data. However, for comparison, the correlations between nodal evolutionary
314 expansion and graph metrics following weighting by Euclidean distance are shown in SFig. 2.

315

316 **Control analyses**

317 Three series of additional control analyses were carried out to test whether the observed
318 effects were consistent across different analytic choices. First, we performed the state-
319 dependent coupling analyses on edge weights directly, i.e. avoiding the step of mapping
320 weights to lengths. Rather than estimating *closeness centrality*, here we conceptualized a
321 node's centrality as its average correlation to all other nodes in the parcellation (see SFig.
322 6B). SFig. 7B depicts the same analyses performed on data not weighted by Euclidean
323 distance between nodes.

324 In a second set of control analyses, we estimated task-state functional connectivity using
325 time-series correlations rather than correlational PPI. Here, data from both task-state runs
326 were preprocessed and analyzed in a similar fashion as the resting-state data. This resulted
327 in two functional connectivity graphs (one per run) per participant, which were averaged
328 before being compared with the resting-state data (see SFig. 6C and the associated caption).
329 SFig. 7C depicts the same analyses performed on data not weighted by Euclidean distance
330 between nodes.

331

332 The third set of control analyses involved the regression of motion estimates (mean absolute
333 and relative motion) from the functional connectivity graphs in the developmental sample
334 before comparing relative coupling of high-expanding nodes across age groups. Regression
335 was performed across subjects at the edge-level (i.e., all region-to-region connectivity
336 estimates were corrected). The relevant results following motion regression are shown in
337 SFig. 8.

338

339 Across all presented analyses, all tests were two-tailed.

340

341 **Results**

342 **High-expanding cortex has broad functional connections and is engaged flexibly across** 343 **different cognitive tasks**

344 First, we tested whether high-expanding nodes communicate more broadly across human
345 functional brain networks than low-expanding nodes. Investigations in the macaque monkey
346 have demonstrated strong positive relationships between dendritic complexity at the
347 microscale neuronal level, and broadness of cortico-cortical neuronal connectivity profiles at
348 the macroscale network level (Scholtens et al. 2014). Therefore, we tested whether high-
349 expanding nodes are characterized by high *participation coefficients*, a graph theoretical
350 measure that quantifies the degree to which a node participates in many of the brain's
351 subnetworks (Guimerà and Nunes Amaral 2005). Functional connectivity between nodes
352 covering the entire cerebral cortex was calculated from resting-state functional MRI (rsfMRI)
353 data from 221 healthy young adults. We estimated optimal community structures, i.e. the
354 brain's subnetworks, through modular decomposition of the group-averaged connectivity
355 graph thresholded at different edge densities (SFig. 1a&b). Next, for each threshold, we
356 calculated every node's participation coefficient – a high value indicating that it connects
357 functionally outside its own community. Finally, we extracted average nodal expansion
358 between three non-human simian primates and humans from estimates of evolutionary
359 cortical scaling (Chaplin et al. 2013) (Fig. 1a). A positive relationship was found between
360 nodal participation coefficient values and estimates of evolutionary expansion at all edge
361 densities (Fig. 1b and SFig. 1c), suggesting that high-expanding regions function as
362 integrative connector nodes in the information flow between more specialized modules in
363 human cortex (Power et al. 2013). In line with this observation, nodal *betweenness centrality*

364 also correlated positively with expansion (SFig. 1c), demonstrating that high-expansion
365 regions often participate in the shortest, most efficient, functional path between any two
366 other nodes in the brain network (Rubinov and Sporns 2010).

367

368 Next, we tested whether the topologically broad and central functional connectivity profiles
369 of high-expanding nodes – as indicated by high participation coefficient and betweenness
370 centrality, respectively – were reflected in their anatomical centrality relative to the
371 canonical functional networks of the human brain (Yeo et al. 2011). The measure *community*
372 *density* represents the number of different networks present within a given radius from a
373 cortical location (Power et al. 2013). We observed a positive relationship between local
374 surface expansion and community density, indicating that high-expanding parts of the cortex
375 have access to multiple networks present in their immediate vicinity (Fig. 1c). This closeness,
376 both at the anatomical and the network topology-level, between high-expanding parts of
377 the cortex and the brain's different networks, makes high-expanding cortex ideally situated
378 to engage in a variety of cognitive processes. To test this hypothesis, we took advantage of
379 recent work on the BrainMap database, in which data from $\approx 10,000$ fMRI-experiments have
380 been merged to establish brain activity patterns common to specific types of tasks (Yeo et al.
381 2015). We grouped cortical surface locations based on the number of task-types (“cognitive
382 components”) they were associated with, and then compared expansion across these levels
383 of cognitive flexibility. In line with our hypothesis, highly flexible nodes were found
384 predominantly in high-expanding cortex (Fig. 1d).

385

386

387 **High-expanding cortex communicates preferentially with regions engaged by the current**
388 **cognitive demands**

389 The above findings suggest that a key role of high-expanding cortical regions may be
390 integration of different cognitive processes. To test this proposal directly, we estimated the
391 *closeness centrality* of cortical nodes in 105 participants scanned using fMRI during two
392 states: unconstrained rest, and a task-state requiring audio-visuo-motor processing (SFig. 3).
393 Closeness centrality represents the average shortest path-length from one node to all other
394 nodes in a network, and thus indicates how tight the functional coupling of a node is to the
395 rest of the network (Rubinov and Sporns 2010). High-expanding regions showed higher
396 closeness centrality during the task-state than during rest and were also more tightly
397 coupled to the rest of the network than lower-expanding nodes (Fig. 2a). Critically, this was
398 also true when accounting for physical (Euclidean) distance between nodes, demonstrating
399 that the tight functional coupling of high-expanding nodes to the rest of the network during
400 multimodal integration is independent of their physical locations on the cortical surface (Liu
401 et al. 2014) (SFig. 4). The higher closeness centrality during the task-state was distributed
402 across all high-expanding regions (Fig. 2b), suggesting that stronger functional coupling
403 during effortful task-operations is a general property of high-expanding cortex and not
404 driven by a subset of cortical regions.

405

406 To test the key proposal that evolutionary high-expanding cortex play a central role in
407 *supramodal* cognition – and thus interact flexibly with different parts of cortex depending on
408 particular cognitive demands – we calculated functional coupling change (resting-state to
409 task-state) between high-expanding regions and all cortical nodes. During the multimodal
410 task-state, their coupling increased (i.e. path length decreased) most prominently with

411 posterior visual perceptual regions, auditory cortex and motor cortex (Fig. 2c). In support of
412 the hypothesis that high-expanding cortex connects with regions engaged during a given
413 cognitive state, these regions also showed upregulated functional coupling between
414 themselves during the task state when compared with rest (Fig. 2d). Critically, medial
415 temporal cortex and ventromedial prefrontal cortex, regions found to be involved in
416 memory consolidation processes during offline rest (van Kesteren et al. 2010; Euston et al.
417 2012), showed the opposite pattern: stronger functional coupling with high-expanding
418 cortex during rest than during the task state (Fig. 2c). Moreover, and in direct accordance
419 with the proposal that evolutionary high-expanding cortex interact flexibly with regions
420 engaged in a given cognitive state, functional coupling between these regions was
421 upregulated during rest when compared with the task-state (Fig. 2d).

422

423 **Human development of neocortical functional coupling patterns follows evolutionary** 424 **expansion trajectories**

425 Recent investigations of neocortical morphometry have found similarities between cortical
426 expansion in human development and primate evolution (Fjell et al. 2015). Evolutionary
427 high-expanding cortex, in particular, shows protracted development, and undergoes larger
428 increases in surface area between infancy and adulthood than lower-expanding regions (Hill
429 et al. 2010; Amlien et al. 2016). Notably, this pattern of surface change during development
430 is more pronounced in high-intelligence samples (Schnack et al. 2015), lending support to
431 the idea that similar developmental and evolutionary trajectories of neocortical change –
432 albeit at very different scales – may promote the same phenotypic characteristics of higher
433 intellectual abilities and supramodal cognition.

434

435 To test whether such correspondence exists between neocortical evolution and functional
436 supramodal cognition characteristics in human cortical development, we collected task-state
437 fMRI data from 46 children and adolescents (6-17 years of age, one excluded due to
438 excessive motion), and compared closeness centrality estimates from regions differing in
439 evolutionary expansion. As found in the adult sample, high-expanding regions' closeness
440 centrality was higher during the multimodal task state also in the children when compared
441 with lower-expanding parts of cortex (Fig. 3a). Additionally, an interaction was observed
442 between age group and regional expansion, indicating that the relative coupling differences
443 between higher- and lower-expanding regions change during development. Specifically,
444 high-expanding cortex' closeness centrality relative to the typical (average) centrality across
445 all nodes, i.e. its relative coupling, was found to be less developed in the young sample when
446 compared with the adults (Fig. 3a). Importantly, less-expanding regions did not show
447 significant differences in coupling between the two age groups. This observation fits well
448 with recent reports of protracted surface area development of evolutionary high-expanding
449 regions, reaching maximum expansion in adolescence (Amlien et al. 2016; Walhovd et al.
450 2016), and suggests that their roles as multimodal integrating hubs follow related
451 developmental trajectories.

452

453 Finally, if evolutionary factors have shaped ontogenetic cortical development, we would
454 expect the mature human brain to reflect the changes that have occurred in primate
455 evolution to a higher degree than the immature brain (e.g. Rakic 2009). For all 150
456 participants in the adult and development sample, we calculated task-state closeness
457 centrality for each of the 170 nodes in the custom neocortical parcellation and correlated
458 these with evolutionary expansion estimates for the same nodes. Next, we fitted a

459 nonparametric local smoothing model (Fjell et al. 2010) to delineate the age trajectory of the
460 relationship between closeness centrality and evolutionary expansion. The relationship was
461 found to be not significant until approximately eighteen years of age, at which point the fit
462 revealed positive correlations between neocortical functional coupling pattern and
463 expansion (Fig. 3b). Interestingly, and in line with previous morphometric reports (Fjell et al.
464 2015; Schnack et al. 2015), participants showing higher similarity between their nodal
465 centrality maps and the evolutionary expansion map were characterized by higher scores on
466 measures of general intelligence (Fig. 3c). This suggests that evolutionary concepts
467 resonating in the functional coupling of the human neocortex are relevant for the
468 characteristic human phenotype of higher intellectual function.

469

470 **Control analyses**

471 The control analyses (presented in SFig. 6-8) supported the main findings reported above.
472 One discrepancy was however observed: when analyzing task data following the resting-
473 state analysis approach (SFig 6C+7C), we did not observe stronger coupling between high-
474 expanding cortex and medial temporal / ventromedial prefrontal cortex during rest when
475 compared to the multimodal task-state. We suspect this may be due to the task time series
476 also containing long periods of rest during the inter-trial intervals. While these inter-trial rest
477 periods were effectively excluded in the main analyses using the correlational PPI approach,
478 they remained present in the control analyses since functional connectivity here was defined
479 as correlations between BOLD time-series covering the full task runs, i.e. without
480 discriminating between state changes within the runs.

481 **Discussion**

482 Our findings point to a central role of evolutionary high-expanding cortex in integrative
483 operations during a variety of cognitive states. The functional signature of such supramodal
484 cognition matures throughout childhood, suggesting that the high-expanding regions
485 develop their characteristic of broad functional connections to many of the brain's networks
486 in tandem with the emergence and refinement of central human cognitive skills. Their
487 postulated overarching function in facilitating supramodal and flexible cognition is
488 supported by the reported links between general intelligence and surface area of high-
489 expanding regions (Fjell et al. 2015; Schnack et al. 2015). Moreover, the functional
490 connectivity 'fingerprints' of high-expanding cortex have been shown to be highly variable
491 from participant to participant, and these characteristic overlaps well with the degree to
492 which a brain region can be used to predict performance during different types of cognition
493 (Mueller et al. 2013). The underlying cellular machinery appears optimized to support such
494 supramodal processes: neuromorphological investigations of primate cortex have found
495 more elaborate dendritic layouts in high-expanding compared with low-expanding regions
496 (Elston et al. 1999), and these structural properties are more pronounced in humans than in
497 non-human primates (Bianchi et al. 2013; Geschwind and Rakic 2013; Donahue et al. 2018).

498

499 In the current study, we interpret cortical regions demonstrating the capacity to integrate
500 information from across the brain in a flexible manner as to take part in supramodal
501 cognition. The claim that certain parts of the cortex, and in particular prefrontal regions, play
502 such flexible integrative roles is hardly new (e.g., Goldman-Rakic 1988), however we believe
503 there is novelty in linking these broad functions to evolutionary morphological changes and

504 their candidate behavioral phenotypes. Our results suggest that, when analyzed as a unit,
505 high-expanding cortex shows both integrative and supramodal characteristics. However, the
506 regions constituting the expansion 'hotspots' are spread in a partly discontinuous manner
507 across large portions of the cortex and may show different characteristics and specializations
508 when investigated in a more fine-grained fashion (Chaplin et al. 2013). A fascinating venue
509 for further research could be to collect data on unimodal in addition to multimodal tasks in
510 an attempt to disentangle modality-specific from integrative functions. Specifically, regions
511 showing increased task-related recruitment and/or functional coupling during multimodal
512 states when compared to unimodal states could be said to be integrative, while regions
513 demonstrating differential coupling patterns over varying task-requirements would support
514 supramodal flexibility. The current results suggest that one would find regions fulfilling both
515 criteria primarily within evolutionary high-expanding cortex.

516

517 **Methodological considerations and limitations**

518 While measures of functional connectivity may be reflective of underlying anatomical
519 connectivity (Vincent et al. 2007; Honey et al. 2009; Hermundstad et al. 2013), they are
520 nevertheless estimated from covariations in signal time-series and can thus be affected by
521 mechanisms other than direct interactions between neuronal populations. In the current
522 study, we do not base any conclusions on observations from single edges (i.e., simple
523 bivariate correlations between two regions), but rely on graph theoretical nodal summary
524 measures – such as closeness centrality – and regions' relative roles in the brain network
525 along these measures. Moreover, due to the within-subject nature of our coupling analyses,
526 we base our conclusions about high-expanding cortex and supramodality on the observed
527 consistent *modulations* in functional coupling across states, not the presence/absence of

528 specific connections. It should be stressed that path-based graph metrics, when estimated
529 from functional connectivity networks, are statistical constructs that do not necessarily
530 reflect information flow along anatomical connections in the brain (Rubinov & Sporns, 2010;
531 Smith et al., 2013; Fornito et. al, 2016). The successful use of functional path-length
532 measures as predictors of cognition (e.g., Bassett et al., 2009; van den Heuvel et al., 2009;
533 Kinnison et al., 2012), and observations that such metrics are under genetic control (Fornito
534 et al., 2011; van den Heuvel et al., 2013; Sinclair et al., 2015), suggests that they reflect
535 biologically meaningful processes and network characteristics. At present, however, shortest
536 path-length measures derived from correlation-based functional networks should not be
537 considered as direct anatomical links. In the current study, we observe similar effects when
538 calculating coupling based on raw correlation weights rather than path-length measures
539 (SFig. 6B and 7B). While this suggests that the observed strong centrality of evolutionary
540 high-expanding regions during multimodal cognitive operations is not an artefact of
541 converting weights to lengths, edge-correlation weights have limited interpretability in
542 terms of anatomical pathways as they can reflect both direct couplings between nodes and
543 interactions via intermediate regions (Fornito et al., 2016).

544

545 Some uncertainty is also associated with the reported relationship between nodal
546 participation coefficient and evolutionary expansion (i.e., Fig. 1b) as they were derived from
547 group averaged graphs of functional connectivity and network parcellations of these.

548 Interestingly, recent work on individual-specific network parcellations (e.g., Gordon et al.,
549 2017; Kong et al., 2018) have suggested that the size, location, and spatial arrangement of
550 cortical networks differ (to some degree) between participants. A common observation in
551 these studies seems to be higher intersubject variability in the spatial layout of association

552 networks when compared with sensory-/motor-networks (Laumann et al., 2015; Wang et al.,
553 2015; Kong et al., 2018), in line with the idea that the development of areas in these
554 networks is less constrained by molecular specification steps in early development (Rosa and
555 Tweedale 2005). In principle, the high participation coefficients observed in high-expanding
556 association cortex when calculated from the group averaged graphs – indicating strong
557 functional coupling across networks – could thus in part be reflective of heterogeneity in the
558 network profiles at the individual level. We are not, however, aware that there is any
559 consensus about how to navigate between individual-specific and group-level based
560 network parcellations and interpret the observed topographical discrepancies. As reliable
561 estimates of the participation coefficient at the individual level are hard to establish even
562 with extensive periods of resting-state data per participant (Gordon et al., 2017), we have
563 here tried to take an alternative approach by investigating high-expanding cortex' postulated
564 integrative role using a variety of measures and approaches. Thus, while keeping the
565 important limitations discussed above in mind, we believe our general claims are supported
566 and strengthened by the observed consistencies across modalities (Community Density
567 analyses) and with independent datasets (Flexibility analyses), as well as by the replication of
568 selective increase in high-expanding cortex' functional coupling during multimodal
569 requirements across two independent groups of participants (Developmental Sample
570 analyses).

571

572 The observed correlations between our measures of functional coupling and registered head
573 motion in the developmental sample were mitigated through standardization at the
574 individual data level, and by including individual motion estimates as covariates at the
575 statistical level. Per-individual standardization of closeness centrality coupling measures

576 effectively removed potential global effects of motion (i.e., affecting all regions) on the
577 centrality measures. Importantly, the standardization step also removed all observed
578 significant correlations between motion and centrality measures when investigating regions
579 characterized by different amounts of evolutionary expansion – "expansion bins" –
580 separately. In other words, after removing potential global effects of head motion from the
581 data, no correlation was found between individual differences in functional coupling of high-
582 expanding cortex and motion (nor for any other expansion bin). Nevertheless, we included
583 an additional control analysis in which motion estimates across subjects were aggressively
584 regressed in an edge-wise fashion from the participant graphs in the developmental sample.
585 While the effects reported in Fig. 3a were only marginally influenced by this additional data
586 cleaning step (see SFig. 8), it should be noted that the correction likely affected shared
587 variance between motion and age-normalized participant IQ (Spearman's $\rho = -.24$, $p =$
588 $.005$), and participant age (Spearman's $\rho = -.39$; $p = 7.3e-07$), that is, variables found to be
589 associated with the function and development of high-expanding cortex (Hill et al., 2010;
590 Schnack et al. 2015).

591

592 The present study is based on interpretation of functional data obtained in humans,
593 correlated with estimates of the differential expansion of parts of the cerebral cortex in
594 primate evolution. To date, these estimates have been derived from careful histological
595 reconstruction of single individual brains from different species, followed by computational
596 registration of 3-dimensional models (Chaplin et al. 2013). The reliance of these estimates
597 on individual brains, rather than population averages, represents a possible limitation of the
598 precision of the present analyses. It should be noted, however, that the differences in
599 expansion that underlie our conclusions are very substantial, relative to the likely degree of

600 individual variation, or errors derived from incorrect assignment of cytoarchitectural
601 boundaries. For example, the differential expansion between the most notable expansion
602 'hotspots' (temporoparietal junction, ventrolateral prefrontal cortex, and dorsal anterior
603 cingulate cortex) and other regions, such as the primary visual cortex and parahippocampal
604 gyrus, is as high as 16-fold between macaque and human (Hill et al. 2010), which is well
605 beyond the variation observed in the volumes of cytoarchitectural areas between individuals
606 of a single primate species (cf. Majka et al. 2016; Woodward et al. 2018). Moreover,
607 although quantitative details of the expansion of different cortical nodes vary slightly
608 depending on which species are used for comparison, the locations of the expansion
609 'hotspots' are remarkably stable (Chaplin et al. 2013). Finally, although some controversy
610 remains about the relative expansion of some regions of the cerebral cortex in primate
611 evolution (e.g. frontal lobe; Barton and Venditti 2013; Sherwood and Smaers 2013), it must
612 be noted that the estimates used in the present study are based on quantitative analyses of
613 species to species registration that took into consideration cytoarchitectural boundaries of
614 areas that are well-defined, rather than gross morphological features of the brain; recent
615 studies that also used cytoarchitecture to guide registration have confirmed that differential
616 expansion exists (Mansouri et al. 2017; Donahue et al. 2018).

617

618 **Conclusion**

619 The present results add to existing knowledge by showing how evolutionary high-expanding
620 regions change in their role as communication hubs in different cognitive states, and that
621 this power gradually emerges during childhood and adolescence development.

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842

843 **Figures legends**

844 **Figure 1**

845 **High-expanding cortex has broad functional connections and is flexibly engaged across**
846 **different cognitive tasks.** (a) Estimates of evolutionary expansion for 170 similarly sized
847 nodes covering the right hemisphere. (b) Spearman correlation between node expansion
848 and node participation coefficient. The presented values are averaged across thresholds and
849 ranked – plotted linear relationship thus represent the Spearman correlation. Observed
850 (non-ranked) participation coefficient values scaled between 0 and 0.71. Traditional hub-
851 measures not incorporating integrative aspects of nodal communication (within-module
852 degree, node strength), did not show any relationships with node expansion (SFig. 1c). (c)
853 Density plot showing the Spearman correlation between vertices' normalized community
854 and estimated evolutionary expansion. (d) Violin plots showing the relationship between
855 cortical expansion and cognitive flexibility at the vertex level. Median expansion is shown as
856 horizontal lines. A Kruskal-Wallis test confirmed that expansion differed across flexibility
857 groups. Post-hoc pairwise comparisons demonstrated that cortical locations involved in five
858 or more cognitive components were more expanded than locations involved in four or less
859 components ($p < 1.25e-07$). All reported p-values are corrected for multiple tests.

860

861 **Figure 2**

862 **High-expanding cortex communicates differently depending on the current cognitive**
863 **demands, and preferentially with regions engaged by those demands.** (a) Average
864 closeness centrality for five expansion bins during resting- and task-state (dark blue: 20%
865 least expanding nodes, yellow: 20% most-expanding nodes; intermediate colors:
866 intermediate expansion levels). Following a significant "expansion bin X state" repeated

867 measures ANOVA (Greenhouse-Geisser corrected following a significant Mauchly's test of
868 sphericity: $\chi^2(9) = 129$, $p < 1e-10$), paired-samples t-tests showed significant increase in
869 closeness centrality in task- compared to resting-state for the highest-expanding nodes only:
870 $t(104)=4.27$, $p_{FDR} < 5.0e-04$. (b) Nodes within expansion hotspot regions (indicated by yellow
871 lines) showing significant (paired-samples t-tests, $p_{FDR} < .05$) changes in closeness centrality
872 from rest to task. (c) Nodes showing significant change (paired-samples t-tests, $p_{FDR} < .05$) in
873 functional coupling with expansion hotspots from rest to task across participants. (d) Mean
874 functional coupling between nodes showing negative (blue) / positive effect (yellow) in
875 panel c. Nodes falling within the expansion hotspot regions were excluded when calculating
876 the mean. Nodes more strongly coupled with high-expanding regions during rest (R>T)
877 showed higher coupling with each other during rest than during task: paired-samples t-test,
878 $t(104)=-10.56$, $p_{FDR} < 3.7e-18$. The opposite effect was observed between nodes more
879 strongly coupled with high-expanding regions during the task-state (T>R): paired-samples t-
880 test, $t(104)=13.25$, $p_{FDR} < 4.4e-24$. The presented data have been weighted by Euclidean
881 distance between nodes. Unweighted data show similar effects (SFig. 6A). All reported p-
882 values are corrected for multiple tests. Error bars represent SEM.

883

884 **Figure 3**

885 **Human development of neocortical multimodal coupling patterns follows evolutionary**

886 **expansion trajectories.** (a) High-expanding cortex showed stronger relative coupling than

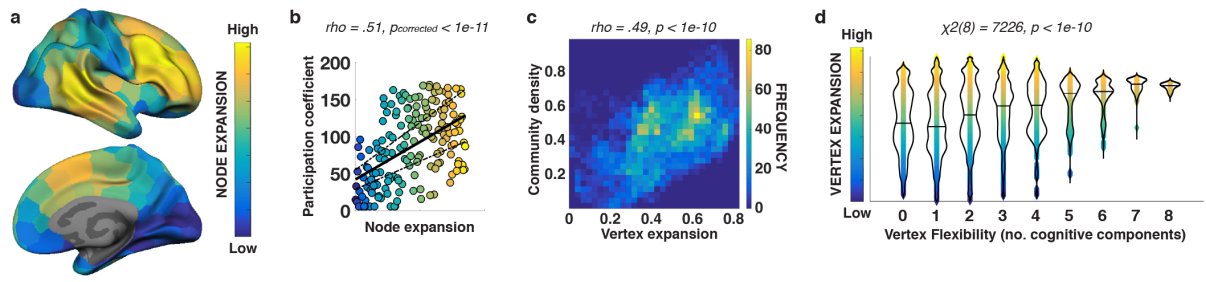
887 lower-expanding regions in both age groups (children: $t(44)>8.09$, $p_{FDR} < 3.0e-10$; adults:

888 $t(104)>23.73$, $p_{FDR} < 1.0e-10$). Following the significant "age group x expansion bin"

889 interaction (Greenhouse-Geisser corrected following a significant Mauchly's test of

890 sphericity: $\chi^2(9) = 63.6$, $p < 3e-10$), post hoc tests showed lower relative coupling of high-

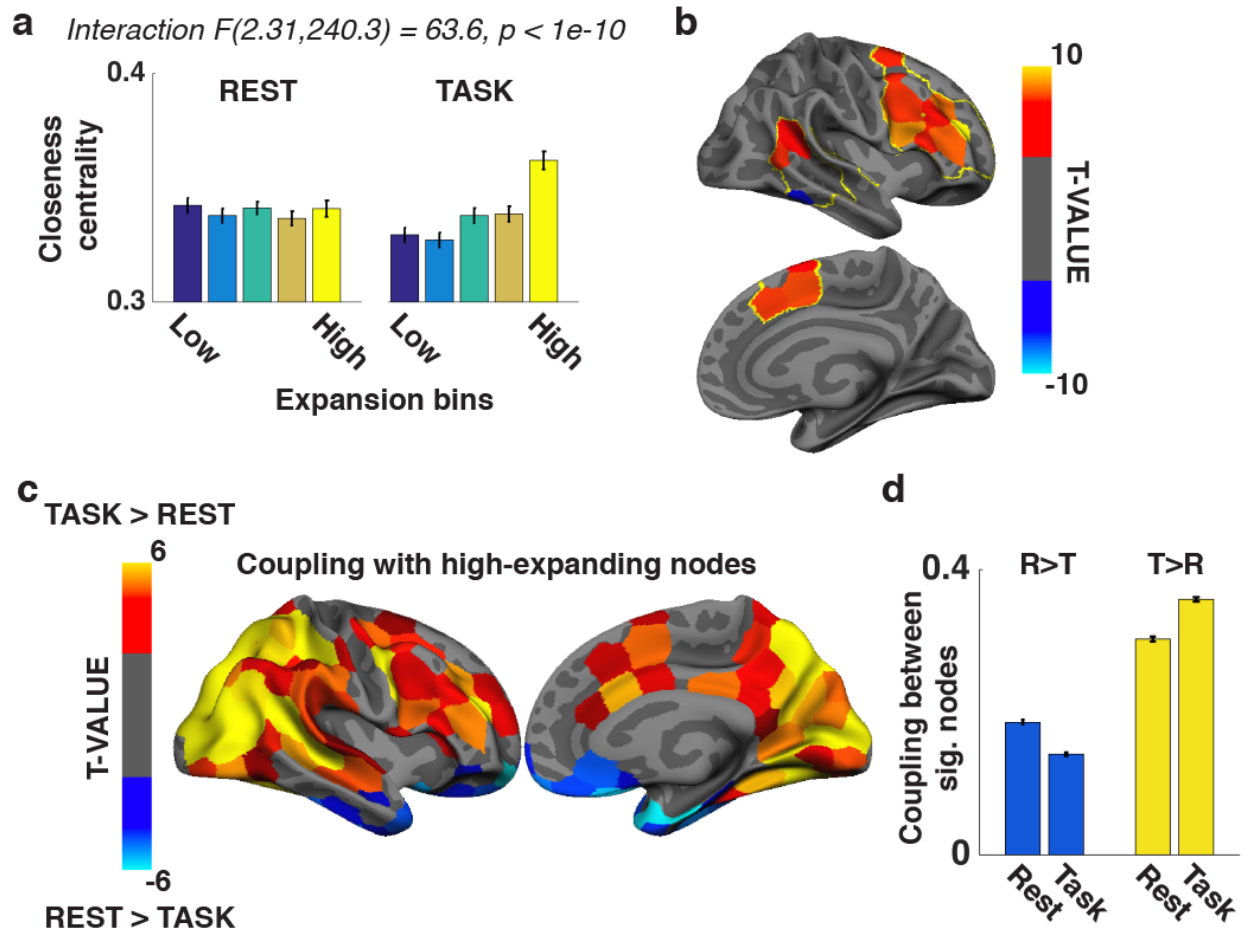
891 expanding nodes in the development sample compared to the adults ($Z = -2.68$, $p_{FDR} < .037$;
892 Wilcoxon rank sum due to unequal variances across groups: Bartlett's test: $\chi^2(1) = 20.8$, $p <$
893 $6e-06$). Lower-expanding nodes did not show significant differences in relative coupling
894 between age groups ($p_{FDR} > .093$). Error bars represent SEM. (b) Individual correlation
895 between nodal closeness centrality and evolutionary expansion plotted as a function of age.
896 The black line represents the best fitting smoothing spline. Red lines represent the
897 bootstrapped 95% confidence interval of the fit. Blue dotted line shows the correlation
898 coefficient at which a correlation with 169 degrees of freedom is significant at $p < .05$
899 ($abs(\rho) > .151$). (c) First principal component calculated from raw scores on two WASI
900 subtests plotted as a function of age. Spearman correlations revealed significant
901 relationships between this measure of general intelligence and individual differences in
902 closeness centrality-vs-expansion correlation (i.e. correlating data points in Fig. 3b and 3c:
903 Spearman's $\rho = .34$, $p < 4.9e-5$). Importantly, this relationship remained when controlling
904 for nonlinear influences of age using partial Spearman correlations ($\rho = .184$, $p = .030$), and
905 when including motion estimates (in addition to age) as control variables ($\rho = .177$, p
906 $= .039$)
907



908

909 *Figure 1*

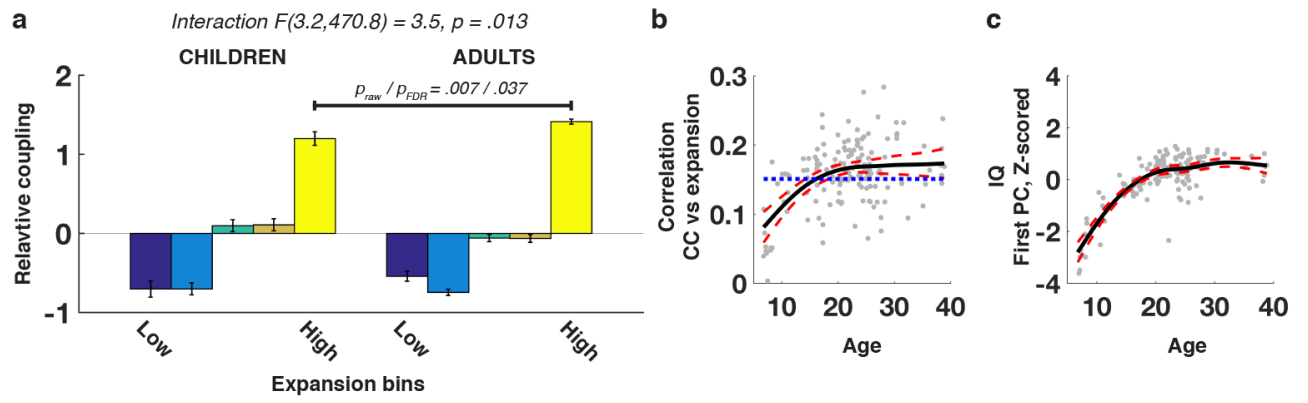
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911

912 *Figure 2*

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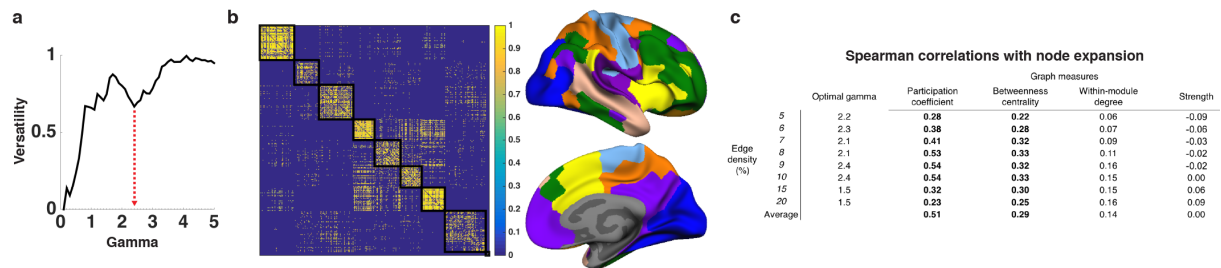
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915 *Figure 3*

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917 **Supplementary Material**

918



919

920 *Supplementary Figure 1.* (a) Versatility (Shinn et al. 2017) was calculated over several resolution parameters for each
 921 thresholded graph (gamma 0.1-5.0 in steps of 0.1). Shown is mean versatility per value of gamma estimated over 500
 922 iterations. The gamma minimizing mean versatility was used as the resolution parameter for modular decomposition of the
 923 thresholded graph, with the additional criterion that the resulting decomposition consisted of more than 3-4 modules. This
 924 last criterion implies a tradeoff weighting network resolution over decomposition stability, and was included to promote
 925 solutions with similar number of modules to what is commonly reported in the literature (Yeo et al. 2011; Power et al.
 926 2013; Bertolero et al. 2015). In the present example (graph thresholded at 10% edge density), gammas below 1.2 were
 927 associated with low versatility (i.e. high stability in estimating communities), however at this resolution level only 3
 928 modules were produced. The next "dip" was found at gamma=2.4, which resulted in a local stable solution consisting of 9
 929 modules. (b) Connectivity matrix thresholded at 10% edge density. Black outlines show the communities resulting from the
 930 modular decomposition - shown in different colors on the cortical surface to the right. (c) Spearman correlations between
 931 estimated network measures and evolutionary expansion per node at different edge density thresholds. Bold numbers
 932 indicate a significant corrected correlation ($p < .05/4$).

933

Graph measures

	Optimal gamma	Participation coefficient	Betweenness centrality	Within-module degree	Strength
5	1.5	0.26	0.30	0.07	0.28
6	1.5	0.31	0.33	0.13	0.28
7	1.4	0.37	0.35	0.21	0.28
8	1.5	0.22	0.31	0.22	0.27
9	1.4	0.31	0.32	0.20	0.26
10	1.4	0.25	0.28	0.19	0.25
15	0.9	0.29	0.28	0.16	0.22
20	1.1	0.23	0.26	0.15	0.19
Average		0.41	0.27	0.17	0.25

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Supplementary Figure 2. Spearman correlations between estimated network measures and evolutionary expansion

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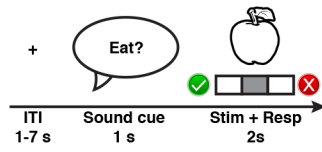
calculated on functional connectivity data after weighting by Euclidean distance between nodes. Bold numbers indicate a

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significant corrected correlation ($p < .05/4$).

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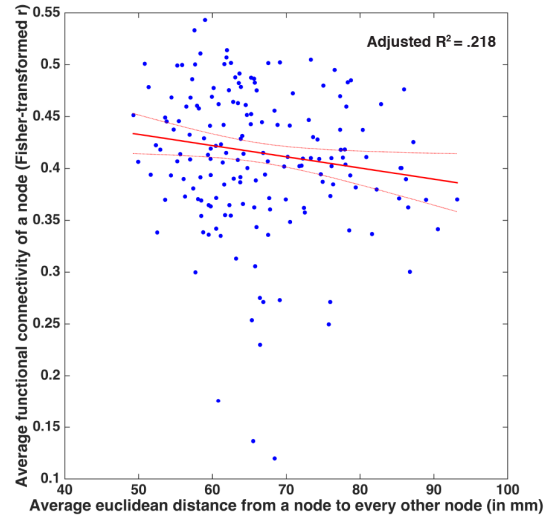
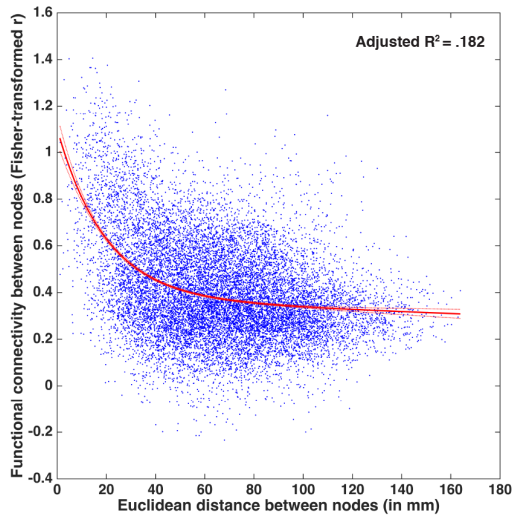
941 *Supplementary Figure 3.* Following a jittered intertrial-interval, an fMRI trial consisted of a voice asking a question ("Can you

942 eat it?" or "Can you lift it?") and the presentation of a drawn object. The participant's task was to indicate with a button

943 press whether the action-item association could be performed or not. See (Sneve et al. 2015) for additional details about

944 the paradigm.

945



946

947 *Supplementary Figure 4.* Left panel: plot showing average functional connectivity across participants between two right-

948 hemispheric nodes from the custom cortical parcellation, as a function of Euclidean distance between the two nodes.

949 Overlaid is a two-term exponential fit, maximizing adjusted R^2 . Edges characterized by short physical distance tend to show

950 higher connectivity than edges representing nodes far apart in physical space. Right panel: plot showing average functional

951 connectivity of a node (mean connectivity across every edge containing a node) as a function of the average physical

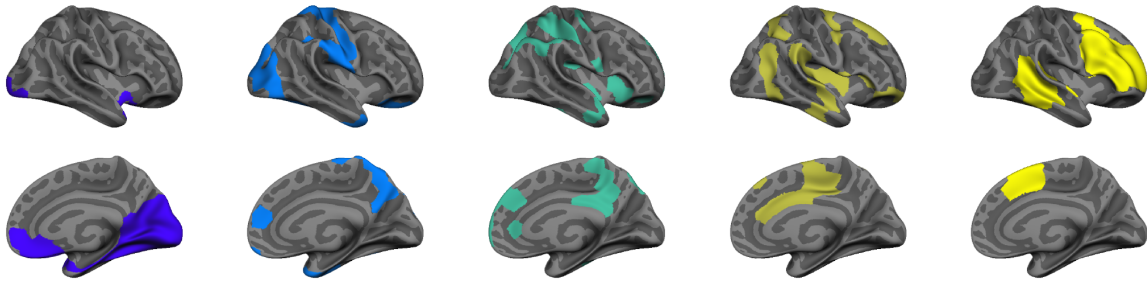
952 distance from that node to all other nodes in the right hemisphere. Overlaid is a robust single-term polynomial fit

953 demonstrating that for nodes with mean global connectivity $> \approx .30$, more centrally placed nodes (in physical space) tend to

954 have stronger global connectivity.

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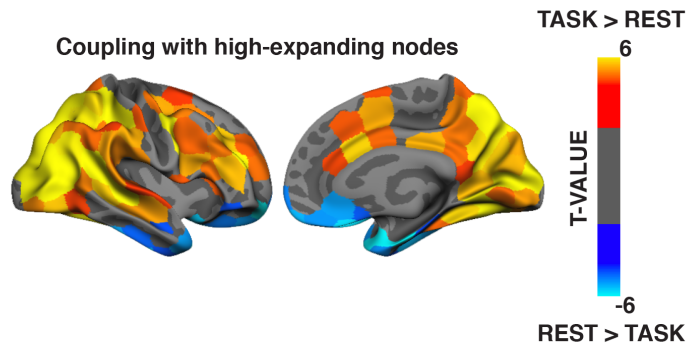
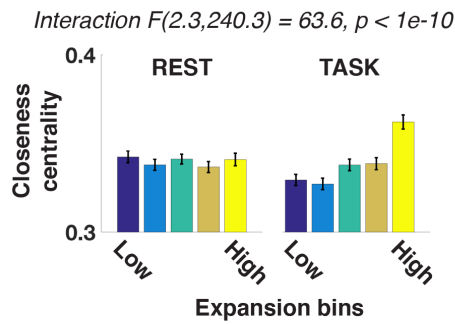
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Bottom 20% expansion bin  Top 20% expansion bin

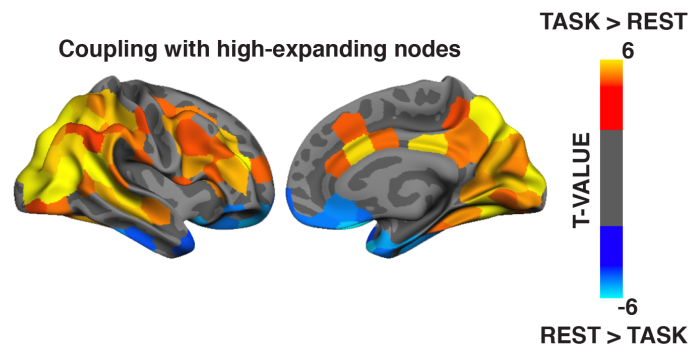
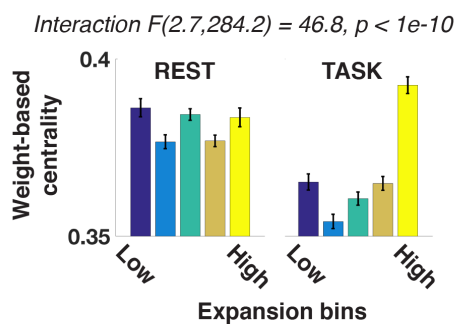
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Supplementary Figure 5. Expansion bins in 20% steps ("Hotspots" in bright yellow to the right)

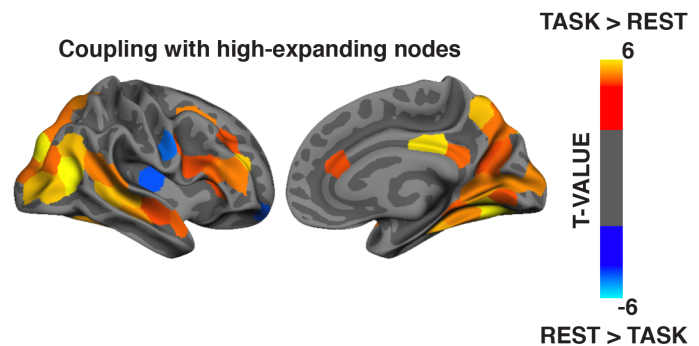
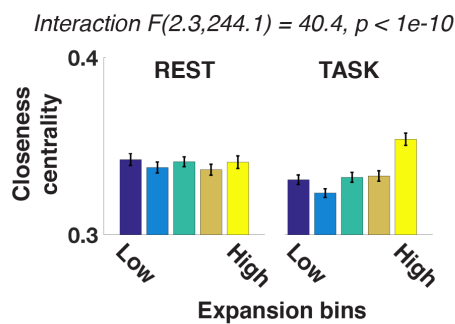
A: Original analyses (as in Fig. 2)



B: “Weight-based” Centrality



C: Closeness Centrality, task-data processed as resting-state data



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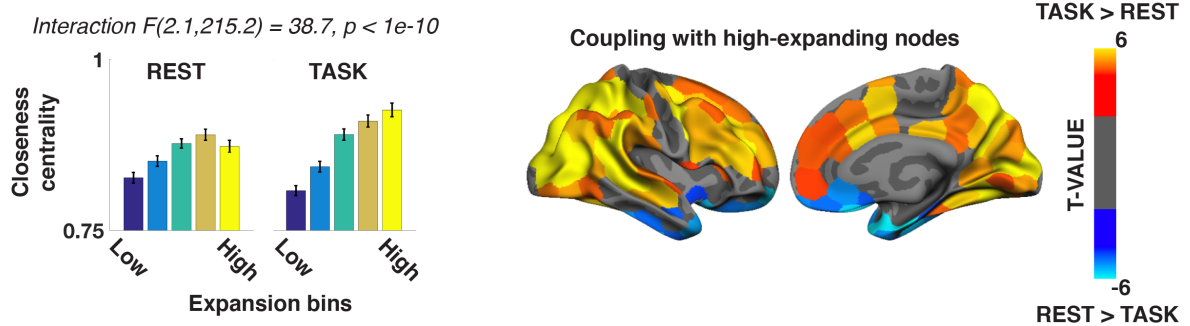
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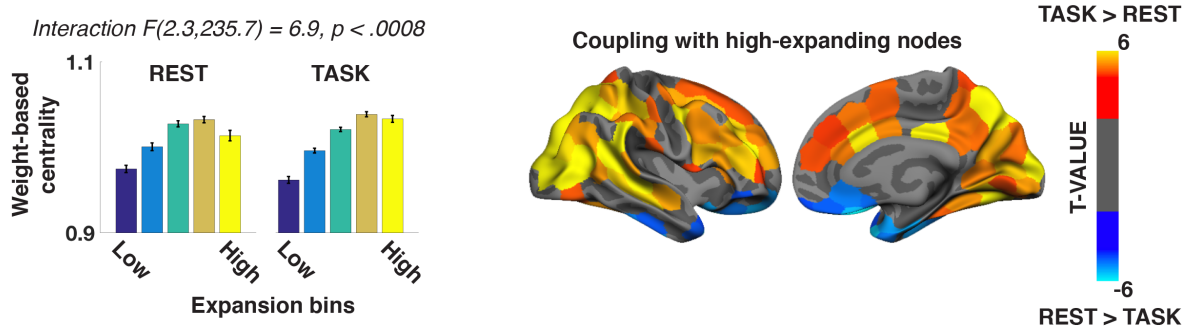
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Supplementary Figure 6. Control analyses on data weighted by the Euclidean distance between nodes. (A) shows the same data as presented in Fig. 2, to facilitate comparisons with the results from control analyses. (B) shows the state-dependent coupling analyses performed on functional connectivity (edge) weights directly, i.e. avoiding the step of mapping weights to path lengths. (C) shows the state-dependent coupling analyses performed following similar pre-processing and analysis of the data from the two states (i.e., analyzing task data following the resting-state analysis pipeline as described in the manuscript, rather than using correlational PPI). Note that, as in the main analyses, edge-wise connectivity weights were normalized by the average weight in the matrix before calculating centrality measures in the control analyses, to allow for comparisons of weighted graph measures from different states (Opsahl et al., 2010).

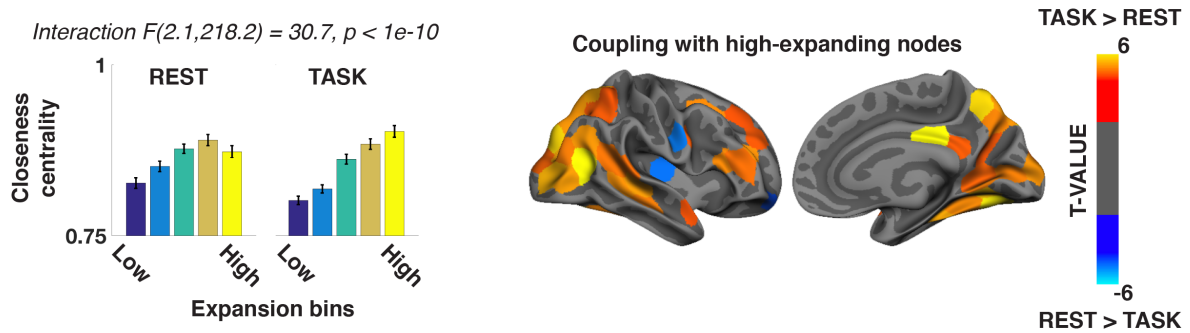
A: Original analyses (as in Fig. 2) – not weighted by Euclidean distance



B: “Weight-based” Centrality – not weighted by Euclidean distance



C: Closeness Centrality, task-data processed as resting-state data – not weighted by Euclidean distance

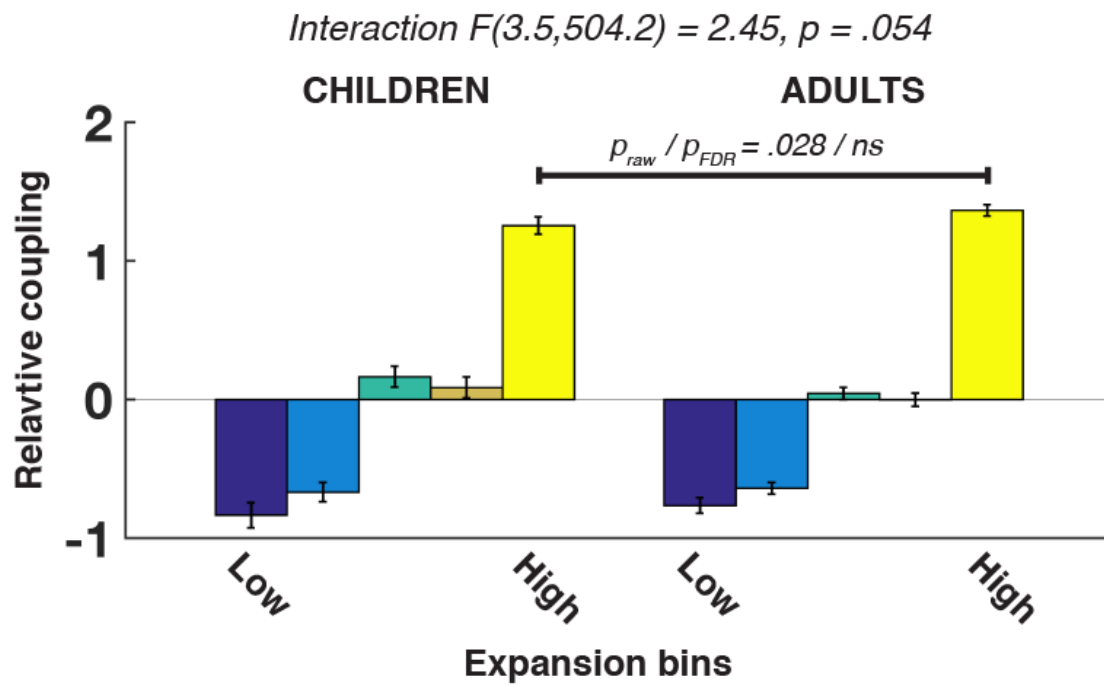


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969 *Supplementary Figure 7. Control analyses on data not weighted by the Euclidean distance between nodes. All analyses were*

970 *performed as described in manuscript Fig. 2 and SFig. 6.*

971



972

973 *Supplementary Figure 8.* Comparison of evolutionary high-expanding cortex' functional coupling across age groups, after
 974 regression of motion measures from the data. Analyses were otherwise performed as described in manuscript Fig. 3. Note
 975 that to calculate FDR-corrected p-values, at least one of the tested p-values has to pass the "Bonferroni-criterion" (in the
 976 current context, .05/5). We therefore only report uncorrected p-values for the post-hoc test comparing relative coupling
 977 between children and adults' high-expanding nodes.

978

979 **Supplementary References**

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